### VIRTUAL JOURNAL CLUB



## Advancing CNS care with digital measures of gait



**Thursday August 7, 2025**11:00 am FT



Melissa Ceruolo

VP, Engineering and Biomarker

Analytics

Medidata



Brett Meyer
Senior Data Scientist, Patient
Experience
Medidata



Reed D. Gurchiek

Assistant Professor, Biomedical

Engineering

Clemson University



Ryan McGinnis

Director, Center for Remote Health

Monitoring & Associate Professor,

Biomedical Engineering

Wake Forest University School of

Medicine



**Benjamin Vandendriessche**Chief Delivery Officer
Digital Medicine Society (DiMe)
Moderator

### But first, housekeeping

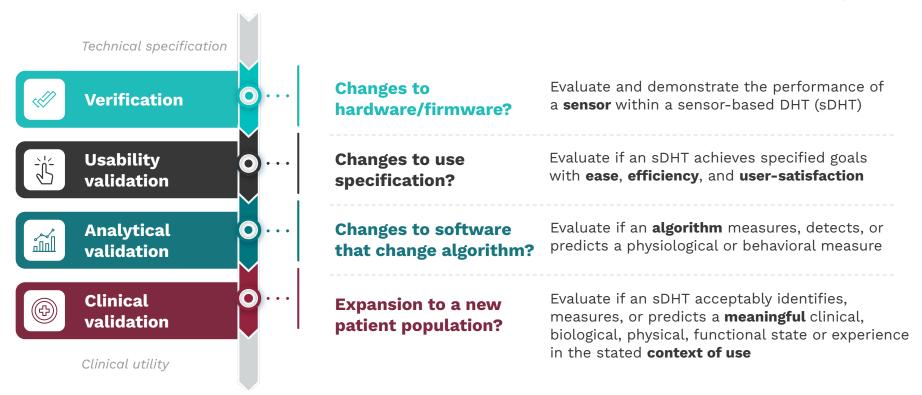


- Today's session is being recorded
- To ask a question for discussion during Q&A, please:
  - Either 'raise your hand' in the participant window and moderator will unmute you to ask your question live, or
  - Type your question into the chat box
- Slides and recording will be available after today's session on <u>DiMe's website</u>.

<u>DiMe Virtual Journal Club</u>

### **V**3 is a modular evaluation process







Validating
Novel Digital
Clinical Measures

An evidence-based framework for rigorous analytical validation and selection of reference measures for both existing and novel digital clinical measures

#### Stage 1

Define

objectives

and gather

initial data



#### Stage 2

Systematically identify the most rigorous reference measure(s)

- Identify existing reference measure(s)
- •
- If necessary, consider developing novel comparator(s)
- **+**

 If necessary, consider identifying anchor measure(s)

#### Stage 3



#### Stage 4

Design a rigorous analytical validation study

- Consider the impact of the data collection environment
- Conduct in-lab and/or in intended use environment analysis

Compile
evidence to
justify claims
and support
regulatory
discussions

### CORE MEASURES of PHYSICAL ACTIVITY



Digital Measures Development

A **core set** of digital clinical measures applicable to the broadest range of therapeutic areas, making it easier to pick the right measure of **physical activity** 



#### **Ontologies**



Walking bout at specified bout durations



Step count



Walking speed



Time spent in MVPA



Measures of postural sway

Source: Physical Activity

### Understanding the Central Nervous System (CNS) Burden



Global Impact on Patients



Sponsor Burden in Alzheimer's









### Trials Still Lack Patient Centricity



~85% of clinical trials is enough patients<sup>1</sup> of clinical trials fail to retain



30%

Average dropout rate across all clinical trials<sup>1</sup>

>66%

of sites fail to recruit a single patient<sup>1</sup> 50%

of sites enroll one or no patients in their studies<sup>1</sup>



### Innovation Through the Patient Lens



Weaving patient and site-centricity from product to the experience level







"Putting the patient first in an open and sustained engagement of the patient to respectfully and compassionately achieve the best experience and outcome for that person and their family."

Technologies developed with patient and site needs at the forefront "If it's not site-friendly, it can't be patient-friendly - because if it doesn't work for the site, it won't be implemented as envisioned for the patient."









### Chest-Based Wearables and Individualized Distributions for Assessing Postural Sway in Persons With Multiple Sclerosis

Brett M. Meyer<sup>®</sup>, Student Member, IEEE, Jenna G. Cohen, Nicole Donahue, Samantha R. Fox, Aisling O'Leary<sup>®</sup>, Anna J. Brown, Claire Leahy, Tyler VanDyk, Paolo DePetrillo, Melissa Ceruolo, Nick Cheney, Andrew J. Solomon<sup>®</sup>, and Ryan S. McGinnis<sup>®</sup>, Senior Member, IEEE



### **Analytical Validation**



by DivE

TABLE II
EYES OPEN POSTURAL SWAY FEATURE CORRELATION

16 persons with multiple sclerosis
(PwMS) performed a two-minute
standing balance assessment on a
force plate.

Chest located sensor offers similar relationships to force plate as previously used and validated sacrum sensor.

Feature	Chest & FP		Sacrum & FP		Chest & Sacrum	
	r	р	r	p	r	p
Jerk	0.88	< 0.01	0.71	< 0.01	0.91	< 0.01
Dist	0.71	< 0.01	0.74	< 0.01	0.58	0.02
RMS	<u>-</u>	X <del>=</del> X	020	=	=	1=1
Path	<u></u>	% <del>=</del> %	) <b>=</b> (	<u>~</u>	<u>~</u>	-
Range	0.60	0.01	0.74	< 0.01	0.94	< 0.01
MV	<u>=</u>	01 <u>-1</u> 0	8 <u>-</u> 8	2	<u>=</u>	8 <u>-</u> 8
MF	0.78	< 0.01	8 <u>-</u> 8	2	<u>=</u>	848
Area	_	_	_	-	_	_
Pwr	_	_	_	-	_	_
F50	-	_	_	-	=	_
F95		6. <del>-</del> .6	( <del>-1</del> )	₹	-	0 <del>.</del>
CF	0.44	0.09	0.59	0.02	0.43	0.10
FD	0.62	0.01	0.63	0.01	0.51	0.04
ApEn	<del>-</del>	N <del>a</del> M	-	=	0.53	0.03
LyExp	-	0 <del></del> (	-	-	-	· -

Significant correlations of postural sway features amongst sensors and force platform (FP) comparisons. Results approaching significance (0.05 are italicized.



### Individualized Distributions



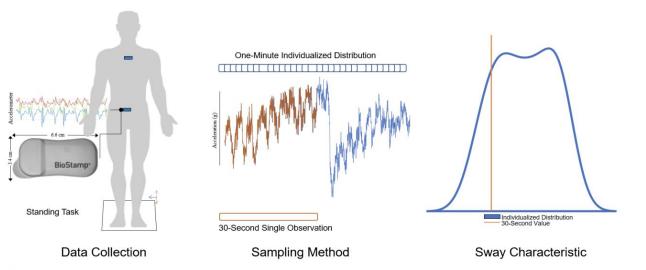


Fig. 1. Process overview of individualized distribution (ID) and a 30-second single observation (SO) methods. Data were collected using wearable sensors located on the chest and sacrum during various standing tasks. Features were computed using ID or SO method. The resulting feature displays the value of an example feature computed using the standard SO method on top of the distribution obtained from the ID method.

N = 39 PwMS

21:18 Faller:Non-Faller

12:27 Male:Female

51 ± 12 y/o

Two minute standing task

Clinical assessment: EDSS

PRO: ABC, MSWS-12, MFIS





# Sway distributions increase strength of relationships to clinical outcomes



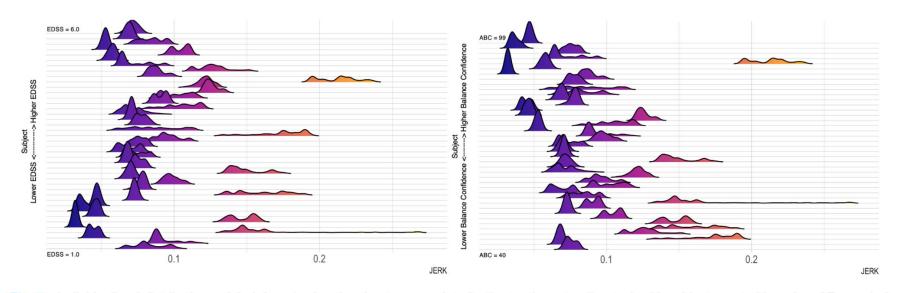


Fig. 5. Individualized distributions of Jerk found using the chest sensor data for the tandem standing task with subjects sorted in order of Expanded Disability Severity Score (EDSS) shown on the left and Activities Specific Balance Confidence Score (ABC) shown on the right. Higher EDSS and balance confidence subjects are at the top of the figures. The strongest correlations were 0.54 and 0.47 for EDSS and ABC with the 5<sup>th</sup> percentile.

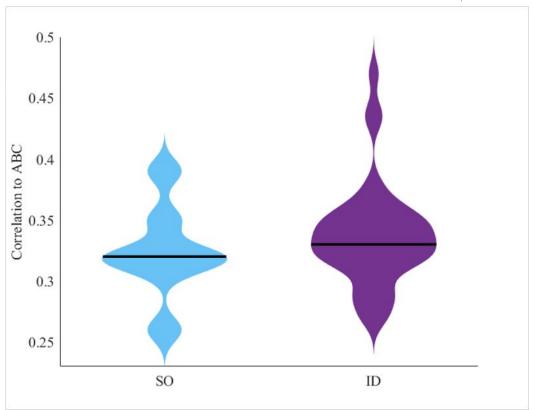






by DivE

# Sway distributions increase strength of relations to PROs







### Accurate Gait Assessment and Reduced Patient Burden from a Chest-Mounted Accelerometer

Brett M. Meyer, *Member, IEEE* Reed D. Gurchiek, Ryan S. McGinnis, *Senior Member, IEEE* and Melissa Ceruolo



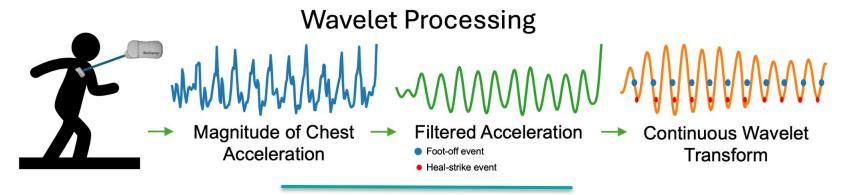
IEEE EMBC 2025 - Proceedings not yet published online





### Methods





N = 10 Healthy Older Adults

Participants wore multiple Biostamp Sensors (including chest)

Participants completed nine ~20foot walks

N = 4 Persons with Huntington's Disease

VICON Motion Capture used for ground truth

Filtering and wavelet analysis to find stride events

Ref: Soltani et al. Algorithms for Walking Speed Estimation Using a Lower-Back-Worn Inertial Sensor: A Cross-Validation on Speed Ranges. 2021





### Methods



- Acceleration calibrated to standing trial
  - Auto-calibration developed and leveraged for use in practice.
- Magnitude heavily filtered using altered 'peak enhancement technique' [1]
- Inspection of initial wavelet transform revealed heel contact events occured at zero-crossing and foot-off events occurred at signal valley.
- Optimization of wave and scale found with a grid search
- Right and Left stride segmented by medial-lateral acceleration

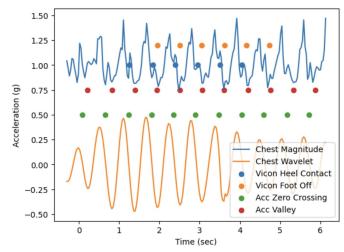


Figure 1. Walking trial with Vicon motion capture stride events (blue and orange dots) plotted over chest magnitude of acceleration (blue). Candidate heel contact (red) and foot off (green) events extracted from wavelet transformed signal

[1]: Soltani et al. Algorithms for Walking Speed Estimation Using a Lower-Back-Worn Inertial Sensor: A Cross-Validation on Speed Ranges. 2021

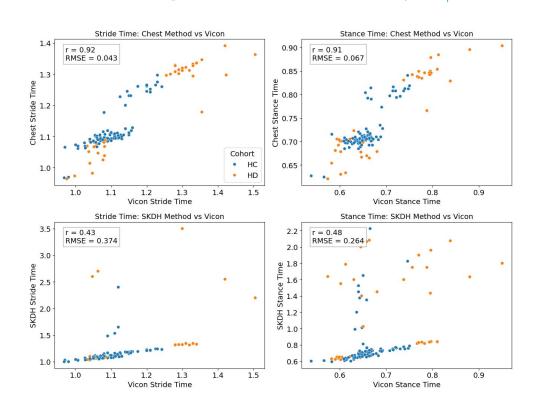




### **Analytical Validation and Comparison**



- Stride event information identified from 126 walks using VICON Motion Capture.
- Computation of stride time, stance time, % stance phase, and double support time.
- Comparison to Chest-scikit digital health (SKDH) performed with optimal parameters.
- Our proposed method vastly outperforms SKDH when considering the full set of walks.







### Stride Length

- Deep learning model utilizes pretraining and transfer learning to find adequate performance from chest sensor.
  - Stride length estimation models from chest
    - Inverted Pendulum: error = 0.13 m
    - Deep learning model: error = 0.11 m
  - DL model offers lower patient and site burden due to lack of patient specific measurements at the expense of additional computation.

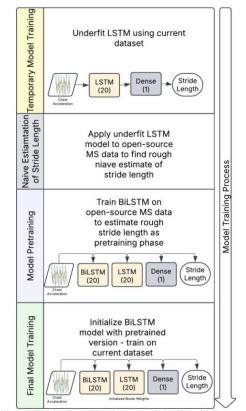


Figure 2. Training flow of deep learning stride length model. Temporary model trained on current healthy and Huntington cohort. Temporary model used to estimate stride length on unseen multiple sclerosis data (Naïve Estimation of Stride Length). Larger model pretrained on multiple sclerosis model. Final model initialized from the pretrained model and trained on current cohort.









IEEE TRANSACTIONS ON NEURAL SYSTEMS AND REHABILITATION ENGINEERING, VOL. 32, 2024

967

# Assessing Free-Living Postural Sway in Persons With Multiple Sclerosis

Brett M. Meyer<sup>®</sup>, *Graduate Student Member, IEEE*, Jenna G. Cohen, *Graduate Student Member, IEEE*, Paolo DePetrillo, Melissa Ceruolo, David Jangraw, Nick Cheney<sup>®</sup>, Andrew J. Solomon<sup>®</sup>, and Ryan S. McGinnis<sup>®</sup>, *Senior Member, IEEE* 

### Passive Sway Analysis



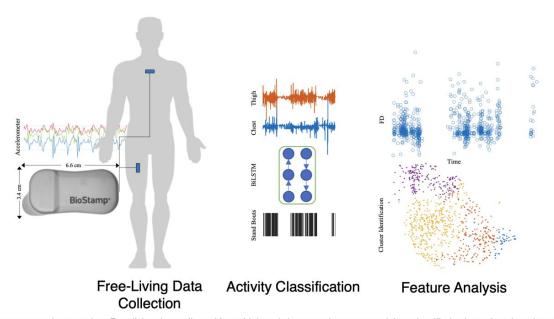


Fig. 1. Data processing overview. Free-living data collected from thigh and chest accelerometer and then classified using a deep learning classifier. Features of postural sway were computed for each standing bout as feature values vary throughout the day and clustering techniques were used to find similar data. BiLSTM: Bidirectional Long-Short-Term Memory network; FD: Frequency Dispersion.

N = 33 PwMS

16:17 Faller:Non-Faller

10:23 Male:Female

 $50 \pm 12 \text{ y/o}$ 

48hr passive sensor wear

Clinical assessment: EDSS

PRO: ABC, MSWS-12, MFIS







### Unique subsets of data exist in free-living sway

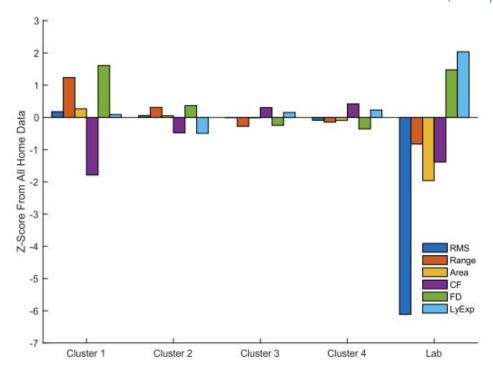


Fig. 4. Z-score differences for each feature between that derived from all remote data and that derived from clustered remote data or lab data.



### Clusters demonstrate radically different relationships



#### Cluster 1

Aggregated Fall Classification Performance:

0.57 AUC, 60% accuracy, 0.63 F1 Strongest Correlation to ABC: -0.57 to CF Strongest Correlation to EDSS: -0.38 to RMS

#### Cluster 2

Aggregated Fall Classification Performance:

 0.71 AUC, 73% accuracy, 0.71 F1 Strongest Correlation to ABC: 0.64 to FD Strongest Correlation to EDSS: -0.55 to FD

#### Cluster 3

Aggregated Fall Classification Performance:

0.53 AUC, 53% accuracy, 0.42 F1 Strongest Correlation to ABC: 0.42 to RMS Strongest Correlation to EDSS: -0.61 to RMS

#### Cluster 4

Aggregated Fall Classification Performance:

 0.16 AUC, 37% accuracy, 0.49 F1 Strongest Correlation to ABC: 0.22 to ABC Strongest Correlation to EDSS: 0.17 (Area/CF)





### COMMON MENTAL HEALTH DISORDERS



Digital Measures Development

+

Developing high-resolution, sensor-generated core digital measures that provide objective, scalable endpoints for common mental health disorders

Join us in transforming mental health research and care



Visit the <u>project page</u> 23

### **THANK YOU**

Melissa Ceruolo | Melissa.Ceruolo@3ds.com

Brett Meyer | Brett.Meyer@3ds.com

Reed Gurchiek | rgurchi@clemson.edu

Ryan McGinnis | rmcginni@wakehealth.edu

Ben Vandendriessche | ben@dimesociety.org



www.dimesociety.org



www.linkedin.com/company/dime-society



bit.ly/DiMe-Slack

